

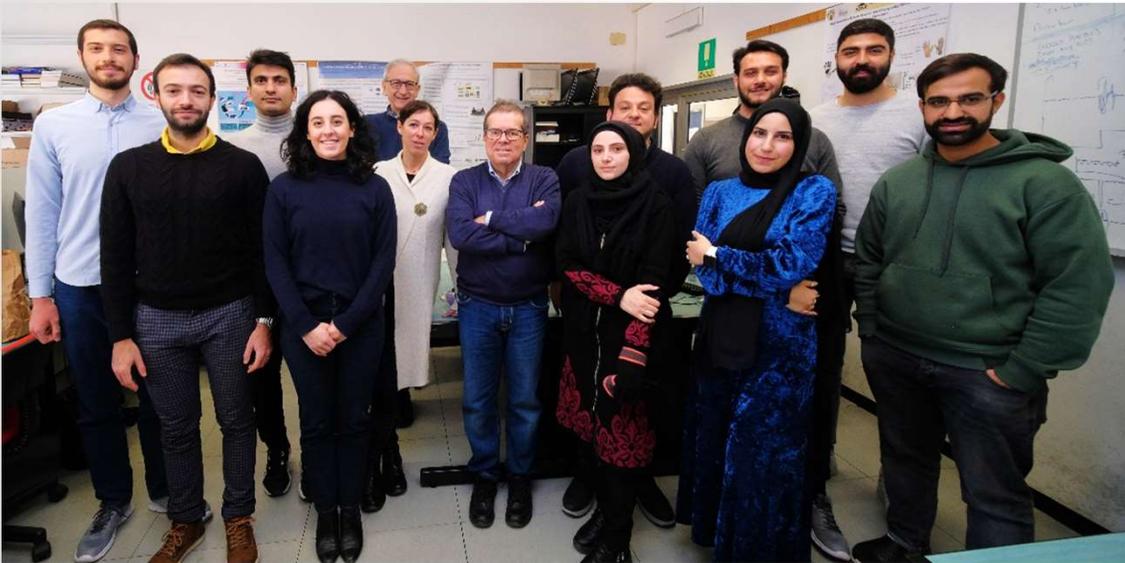
# TOWARDS ARTIFICIALLY RESTORING THE SENSE OF TOUCH



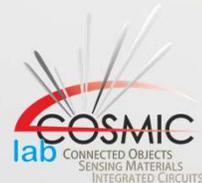
*L. Seminara*

*Electrical, Electronics, Telecomm Engineering and Naval Architecture Department  
University of Genoa, Italy*

# Where we are



# Who we are



▶ **MOTIVATION**

▶ **HUMAN SENSE OF TOUCH**

▶ **ARTIFICIAL SENSE OF TOUCH**

- *Our system*: distributing sensing, electronics, cutaneous electrostimulation
- Clinical applications and *WORK IN PROGRESS*

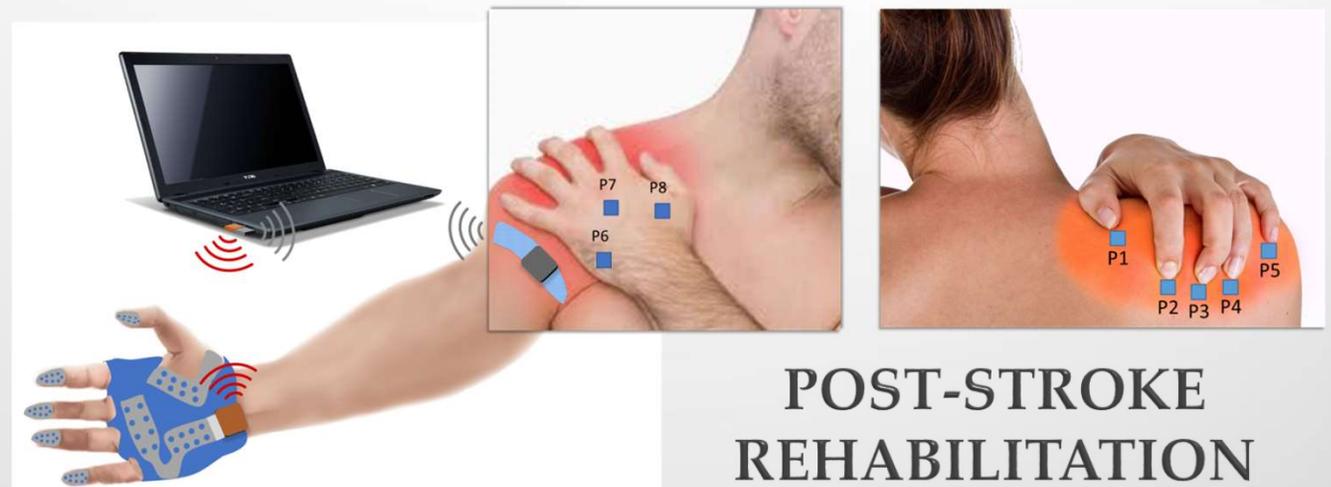
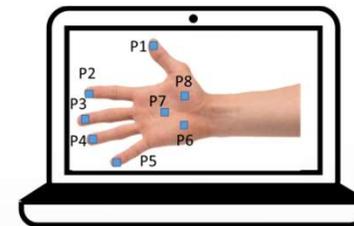
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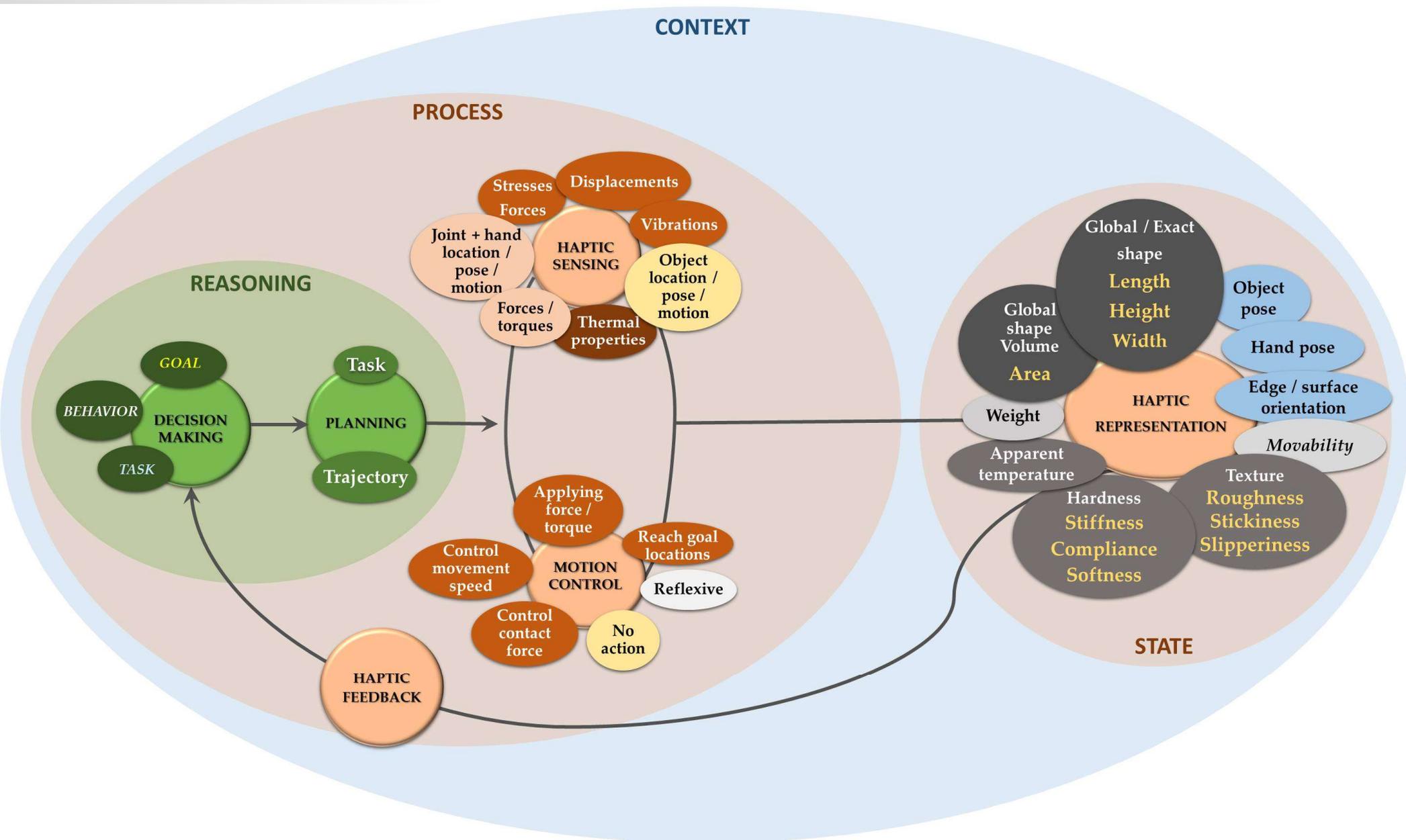
# PROSTHETICS

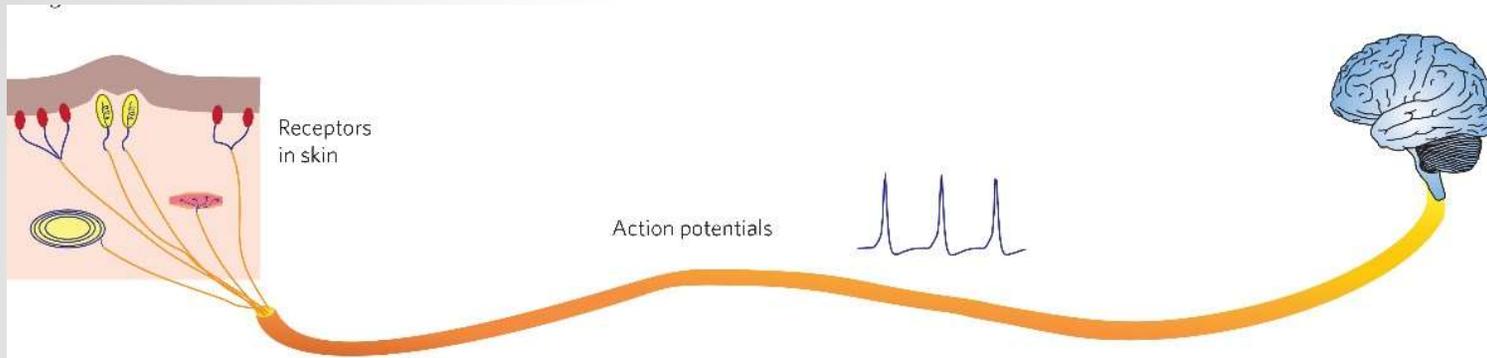


## POST-STROKE REHABILITATION

Nataletti, S., Leo, F., Seminara, L., Trompetto, C., Valle, M., Dosen, S., & Brayda, L. (2020). Temporal asynchrony but not total energy nor duration improves the judgment of numerosity in electrotactile stimulation. *Frontiers in Bioengineering and Biotechnology*, 8, 555.

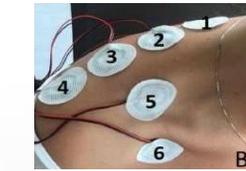
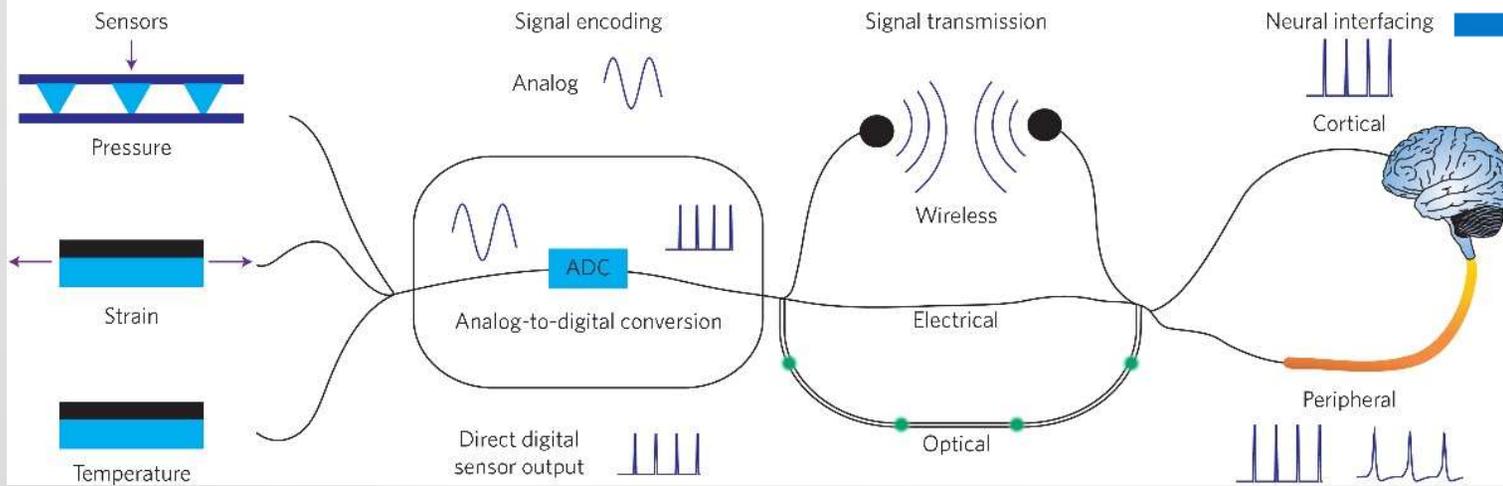
# A complex picture





**cortical neural interfaces** that record / stimulate neurons directly in the **brain**

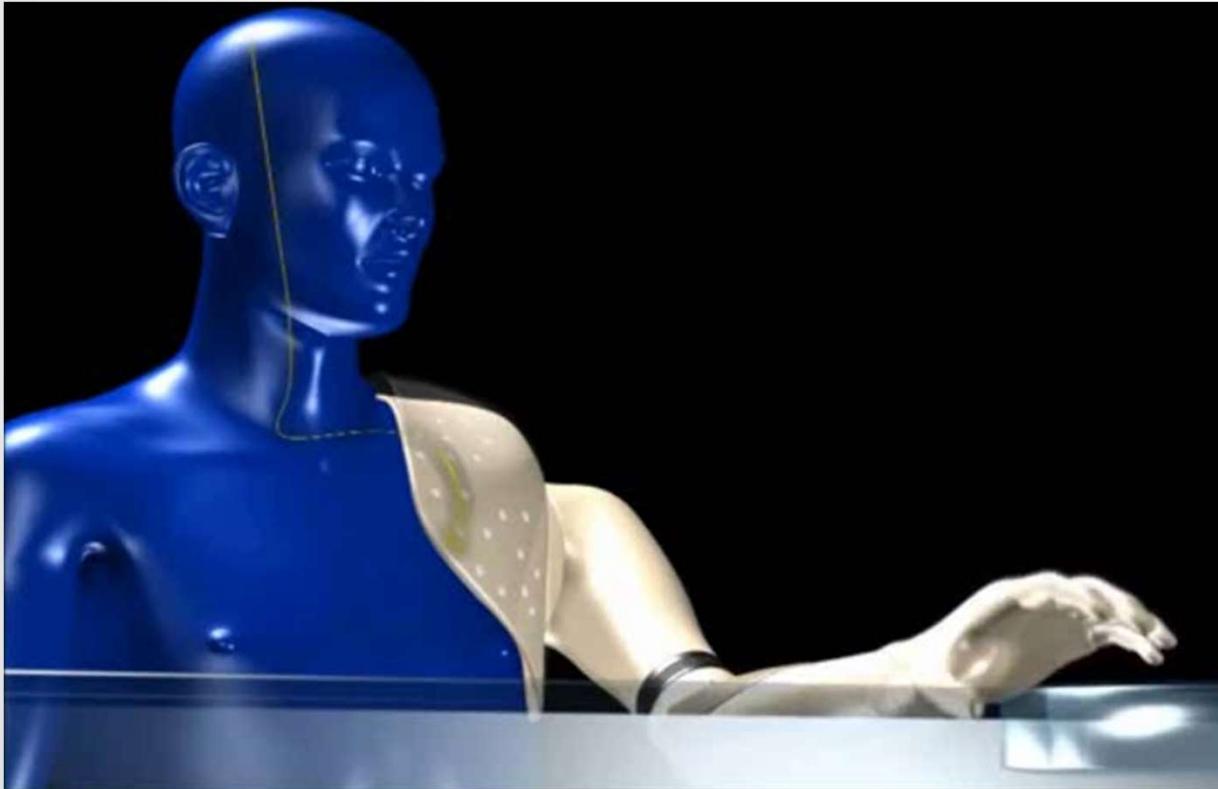
Artificial skin transduction



interface with the **peripheral nervous system**

Chortos, A. L. J. and Bao, Z., «Pursuing prosthetic electronic skin», Nature materials, 2016

# Sensory feedback to the user



UTILITY

EMBODIMENT

# Focusing on the SKIN

The human haptic perceptual system can be conceptualized as a **continuum** organized as a **tensegrity structure**\* modeling the conjunction of muscular, connective tissue, and skeletal structures. In biological systems, touch receptors are intimately connected to this continuum, and the surrounding tissue with its surface properties (e.g., ridges) becomes an extension of the sensor system itself.

→ To artificially reconstruct the sense of touch, a reliable and robust *biomimetic* artificial system integrating **high-density networks of sensing units** is needed

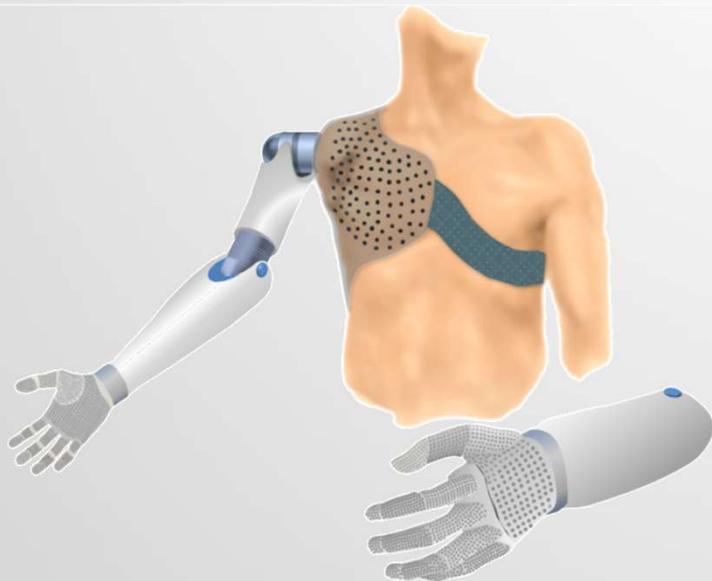
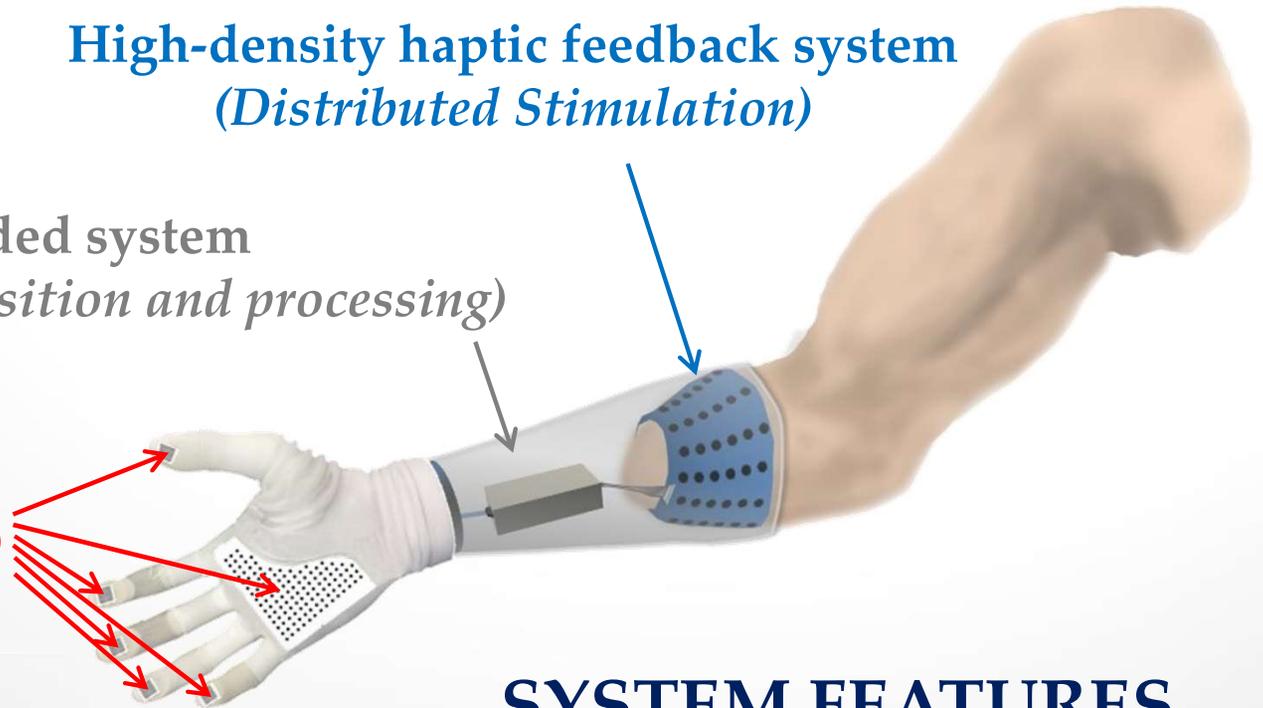
\* M. T. Turvey, S. T. Fonseca, The medium of haptic perception: a tensegrity hypothesis. *J. Mot. Behav.* 46, 143–187 (2014).

# *Non invasive approach - Concept*

**High-density haptic feedback system**  
*(Distributed Stimulation)*

**Embedded system**  
*(Tactile data acquisition and processing)*

**High-density sensor array**  
*(Distributed Tactile Sensing)*



## **SYSTEM FEATURES**

**Wearable:** Small size, not heavy

**Real-time** sensing-stimulation

**Low power consumption**

**Self-powered** device

**Long-life** (daily) device

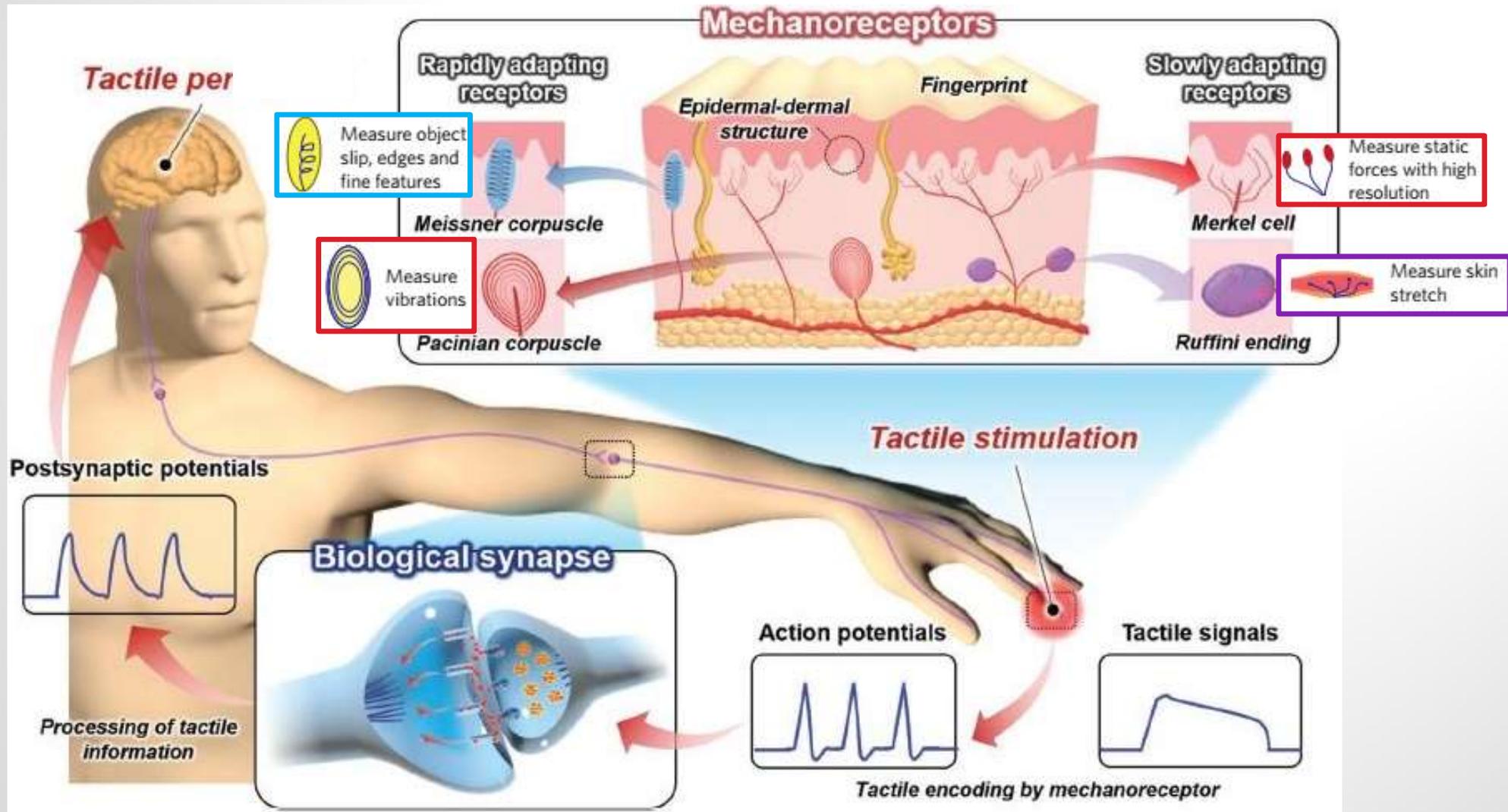
▶ MOTIVATION

▶ HUMAN SENSE OF TOUCH

▶ ARTIFICIAL SENSE OF TOUCH

- *Our system: distributing sensing, electronics, cutaneous electrostimulation*
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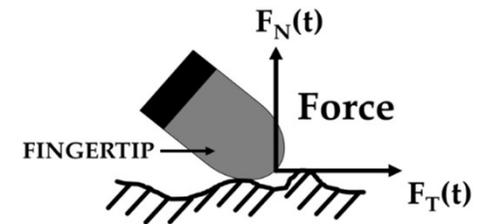
# The whole process of tactile perception in humans



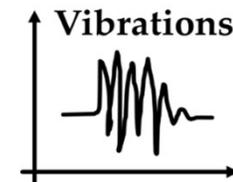
Y. Lee, J. Park, A. Choe, S. Cho, J. Kim, and H. Ko, "Mimicking Human and Biological Skins for Multifunctional Skin Electronics," *Adv. Funct. Mater.*, 2020.



The **sensory function** DOES NOT ONLY depend on the *mechanoreceptor type*, but also on **how** it is integrated into the *whole mechanical structure*.



**DISPLACEMENT**  
(Strain, curvature, stretch)



MECHANICAL and SURFACE PROPERTIES of the HUMAN SKIN (under the spotlight):

- Soft and compliant
- Hyperelastic + viscoelastic behaviour
- Ridges

▶ MOTIVATION

▶ HUMAN SENSE OF TOUCH

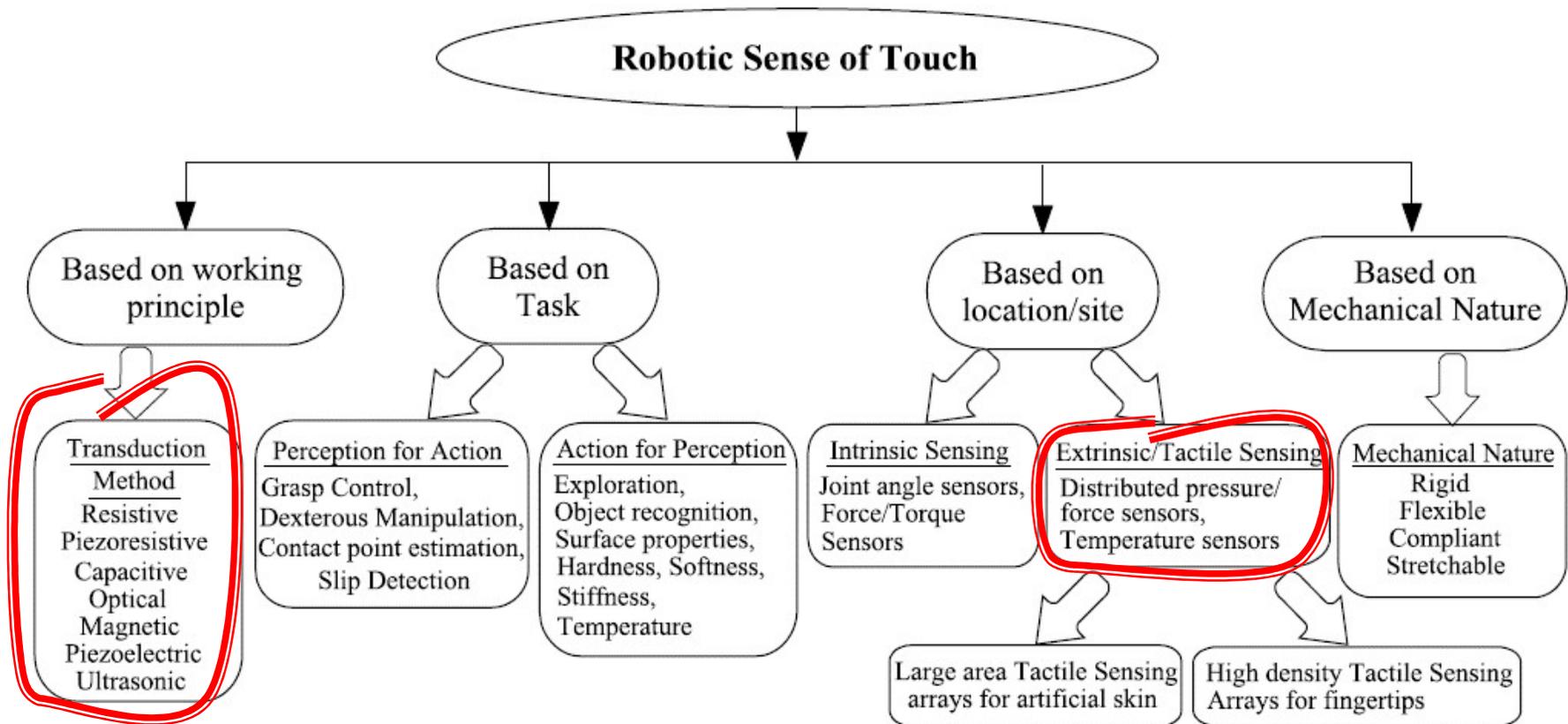
▶ **ARTIFICIAL SENSE OF TOUCH**

- *Our system: distributing sensing, electronics, cutaneous electrostimulation*
- **Clinical applications and *WORK IN PROGRESS***

# Artificial sense of Touch

If we want to understand and, to some extent, replicate human intelligence **we need to understand the technological solutions supporting the biological functions and discover the technologies** which allow such functions to be implemented artificially.

Giulio Sandini, Italian Institute of Technology  
Robotics, Brain and Cognitive Sciences

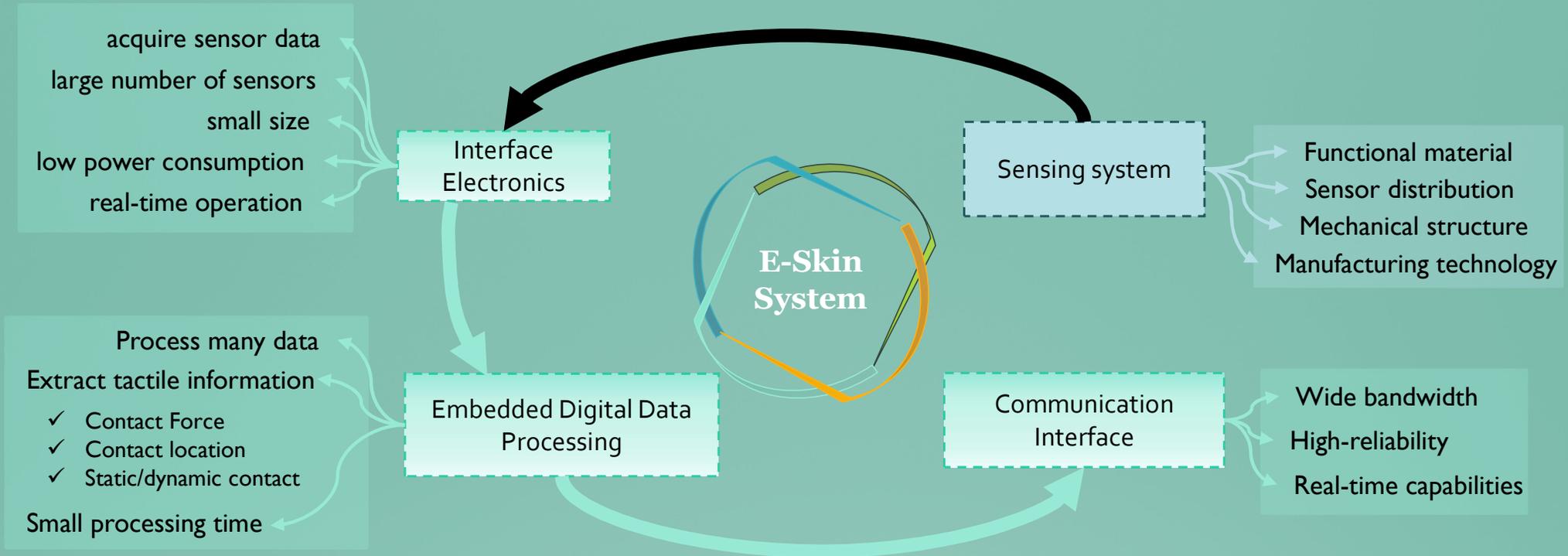


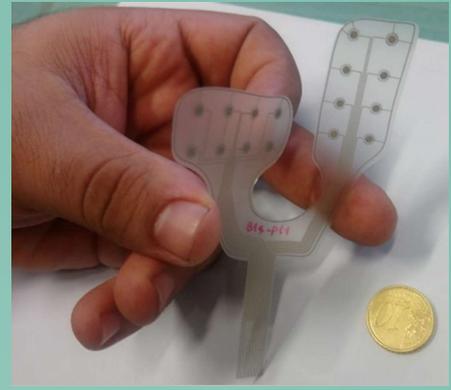
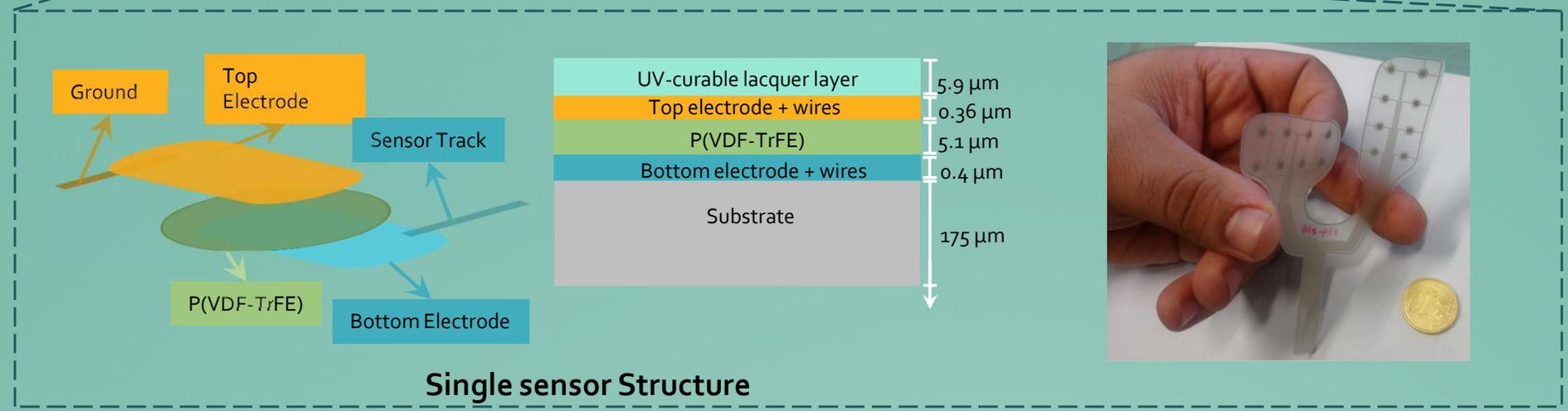
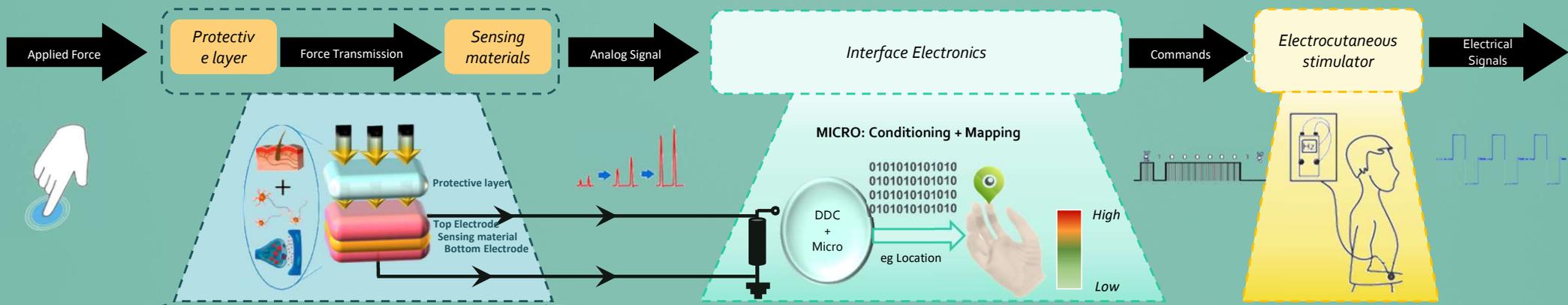
▶ MOTIVATION

▶ HUMAN SENSE OF TOUCH

▶ ARTIFICIAL SENSE OF TOUCH

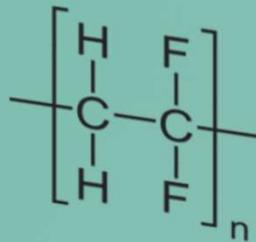
- *Our system: distributing sensing, electronics, cutaneous electrostimulation*
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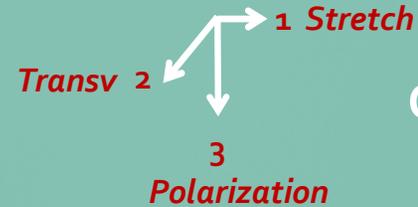


# FUNCTIONAL MATERIAL: PVDF PIEZOELECTRIC POLYMER

PolyViniliDene  
Fluoride



- « Flexible
- « Frequency: <1Hz -1kHz
- « Wide dynamics



ORTHOTROPIC SYSTEM

Polarized PVDF film



Oriented  
molecules

Oriented dipoles

PACINIAN + RUFFINI + MERKEL + MEISSNER

ALL HUMAN SKIN MECHANORECEPTORS

DYNAMIC  
&  
TRANSIENT  
STIMULATION

# THICKNESS MODE

ELECTRICAL  
DISPLACEMENT

$$\begin{bmatrix} D_1 \\ D_2 \\ D_3 \end{bmatrix}$$

OUTPUT

PIEZOELECTRIC  
MATRIX

$$\begin{bmatrix} 0 & 0 & 0 & 0 & d_{15} & 0 \\ 0 & 0 & 0 & d_{24} & 0 & 0 \\ d_{31} & d_{32} & d_{33} & 0 & 0 & 0 \end{bmatrix}$$

STRESS

$$\begin{bmatrix} \cancel{T_{11}} \\ \cancel{T_{22}} \\ T_{33} \\ T_{23} \\ T_{13} \\ T_{12} \end{bmatrix}$$

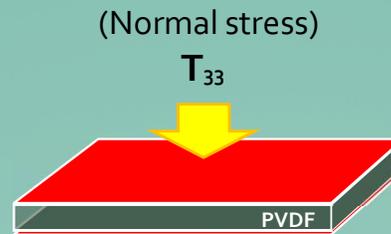
INPUT

PERMITTIVITY

$$\begin{bmatrix} \epsilon_{11} & 0 & 0 \\ 0 & \epsilon_{22} & 0 \\ 0 & 0 & \epsilon_{33} \end{bmatrix}$$

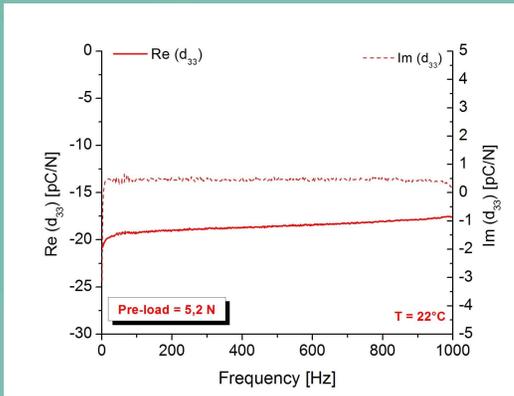
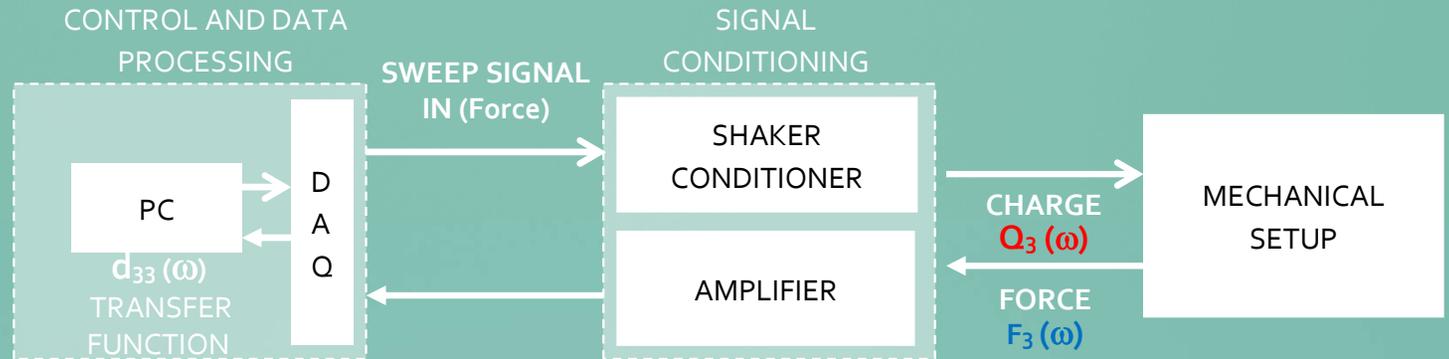
ELECTRIC  
FIELD

$$\begin{bmatrix} E_{ext1} \\ E_{ext2} \\ \cancel{E_{ext3}} \end{bmatrix}$$



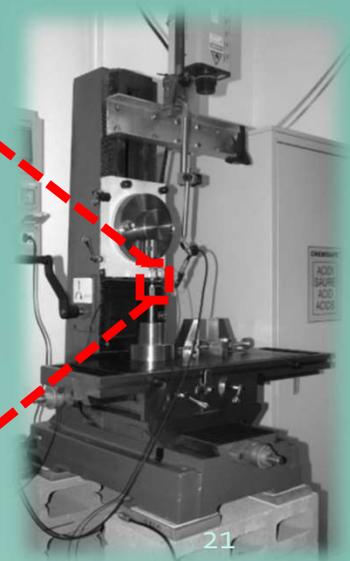
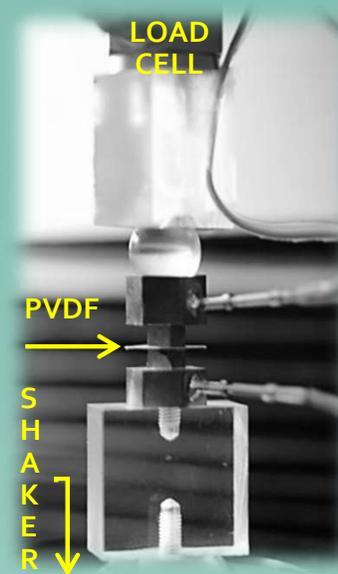
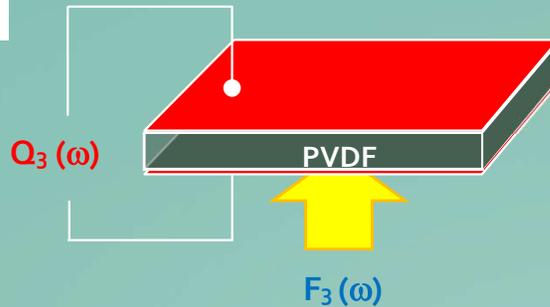
RIGID SUBSTRATE

# EXPERIMENTAL SETUP: THICKNESS MODE



Thickness mode

$$D_3(\omega) = d_{33}(\omega) * T_{33}(\omega)$$

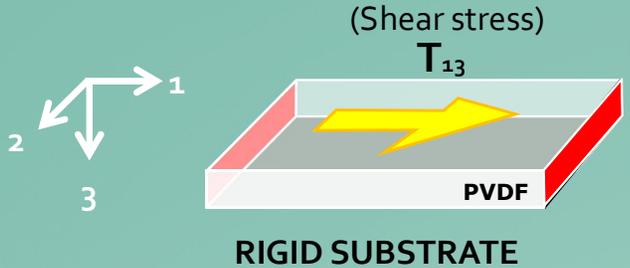


# SHEAR MODES

**ELECTRICAL DISPLACEMENT**      **PIEZOELECTRIC MATRIX**      **STRESS**      **PERMITTIVITY**      **ELECTRIC FIELD**

$$\begin{bmatrix} D_1 \\ D_2 \\ D_3 \end{bmatrix} = \begin{bmatrix} 0 & 0 & 0 & 0 & d_{15} & 0 \\ 0 & 0 & 0 & d_{24} & 0 & 0 \\ d_{31} & d_{32} & d_{33} & 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} T_{11} \\ T_{22} \\ T_{33} \\ T_{23} \\ T_{13} \\ T_{12} \end{bmatrix} + \begin{bmatrix} \epsilon_{11} & 0 & 0 \\ 0 & \epsilon_{22} & 0 \\ 0 & 0 & \epsilon_{33} \end{bmatrix} \begin{bmatrix} E_{ext 1} \\ E_{ext 2} \\ E_{ext 3} \end{bmatrix}$$

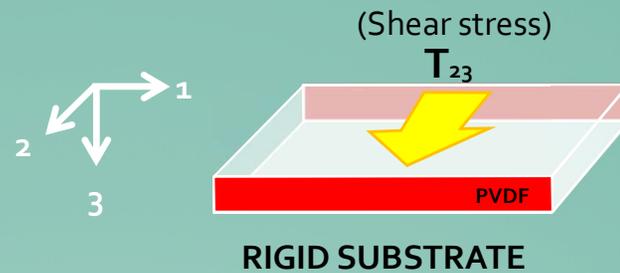
**OUTPUT**      **INPUT**



# SHEAR MODES

$$\begin{array}{c} \text{ELECTRICAL} \\ \text{DISPLACEMENT} \end{array} \begin{bmatrix} D_1 \\ D_2 \\ D_3 \end{bmatrix} = \begin{array}{c} \text{PIEZOELECTRIC} \\ \text{MATRIX} \end{array} \begin{bmatrix} 0 & 0 & 0 & 0 & d_{15} & 0 \\ 0 & 0 & 0 & d_{24} & 0 & 0 \\ d_{31} & d_{32} & d_{33} & 0 & 0 & 0 \end{bmatrix} \begin{array}{c} \text{STRESS} \\ T_{11} \\ T_{22} \\ T_{33} \\ T_{23} \\ T_{13} \\ T_{12} \end{bmatrix} + \begin{array}{c} \text{PERMITTIVITY} \\ \epsilon_{11} & 0 & 0 \\ 0 & \epsilon_{22} & 0 \\ 0 & 0 & \epsilon_{33} \end{bmatrix} \begin{array}{c} \text{ELECTRIC} \\ \text{FIELD} \\ E_{ext1} \\ E_{ext2} \\ E_{ext3} \end{bmatrix}$$

OUTPUT
INPUT

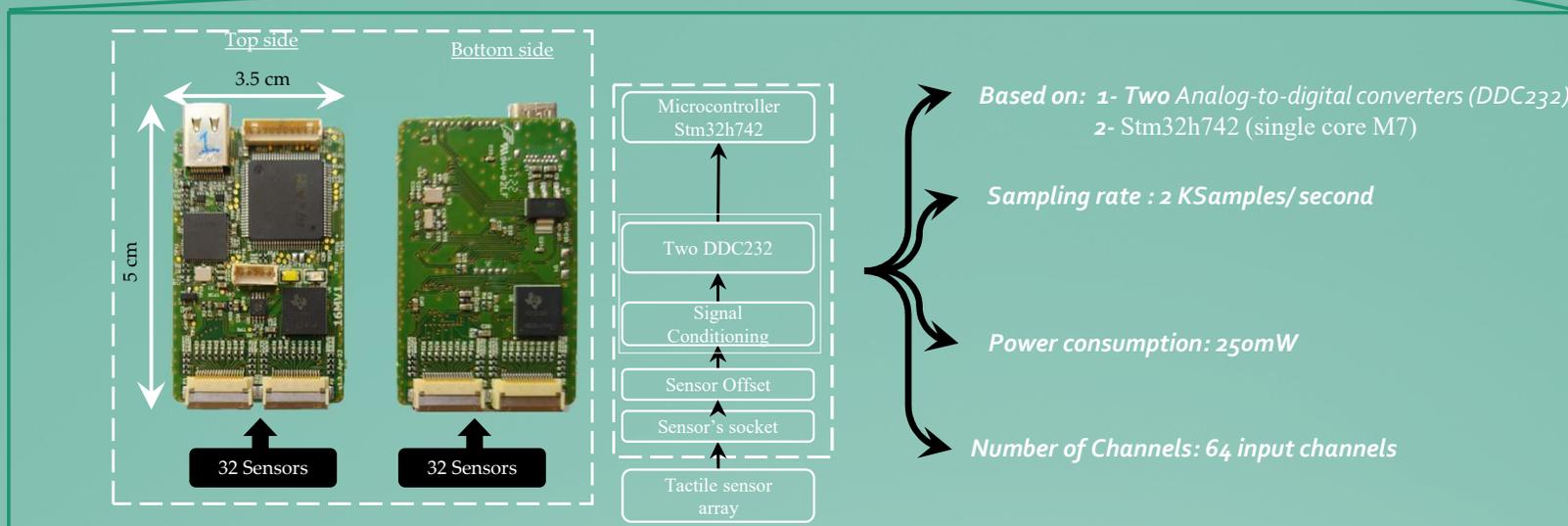
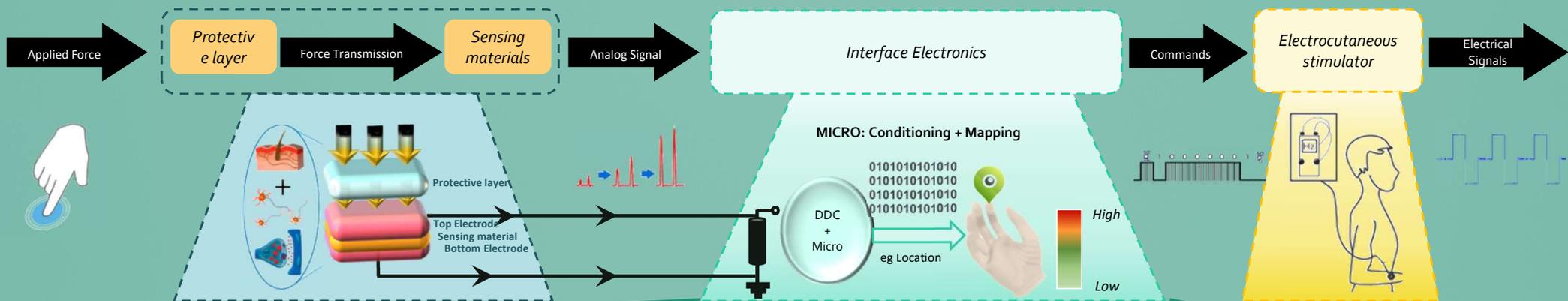


## E-SKIN REQUIREMENTS

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Detectable Force Range	0.01N-10N
Sensor Frequency Bandwidth	< 1 Hz - 1kHz
Spatial Resolution	$\leq 1\text{mm}$ for fingertips 10 – 20 mm for palm
Mechanical Sensor system characteristics	Flexible & conformable Robust & durable
Electrical Sensor system characteristics	Low power Low <i>latency</i> (real-time) Minimal wiring and cross talk

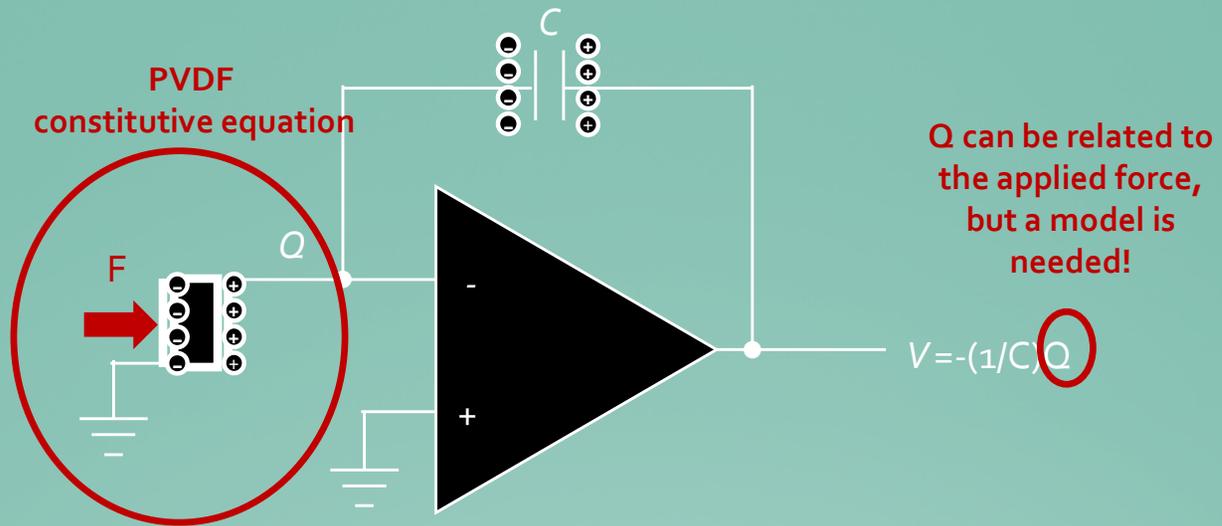
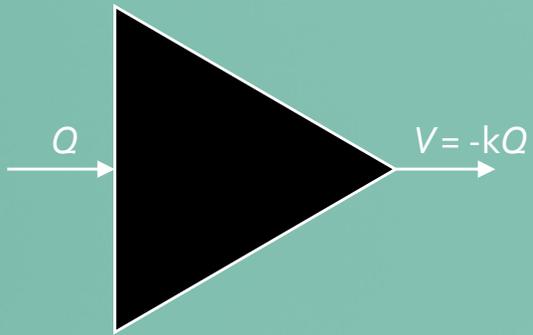
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Abbass, Y., Saleh, M., Dosen, S., and Valle, M., Embedded Electrotactile Feedback System for Hand Prostheses Using Matrix Electrode and Electronic Skin; TBCAS Oct. 2021 912-925

Abbass, Y., Dosen, S., Seminara, L., & Valle, M. (2022). Full-hand electrotactile feedback using electronic skin and matrix electrodes for high-bandwidth human-machine interfacing. *Philosophical Transactions of the Royal Society A*, 380(2228), 20210017.

# CHARGE AMPLIFIER





# FROM CONTACT TO PERCEPTION

ROBOTICS



TACTILE SENSING = detection and measurement of contact parameters in a predetermined contact area + subsequent processing of the signals at the taxel level, i.e., before sending tactile data to higher levels for perceptual interpretation.

TACTILE SENSING = detection and measurement of contact parameters in a predetermined contact area

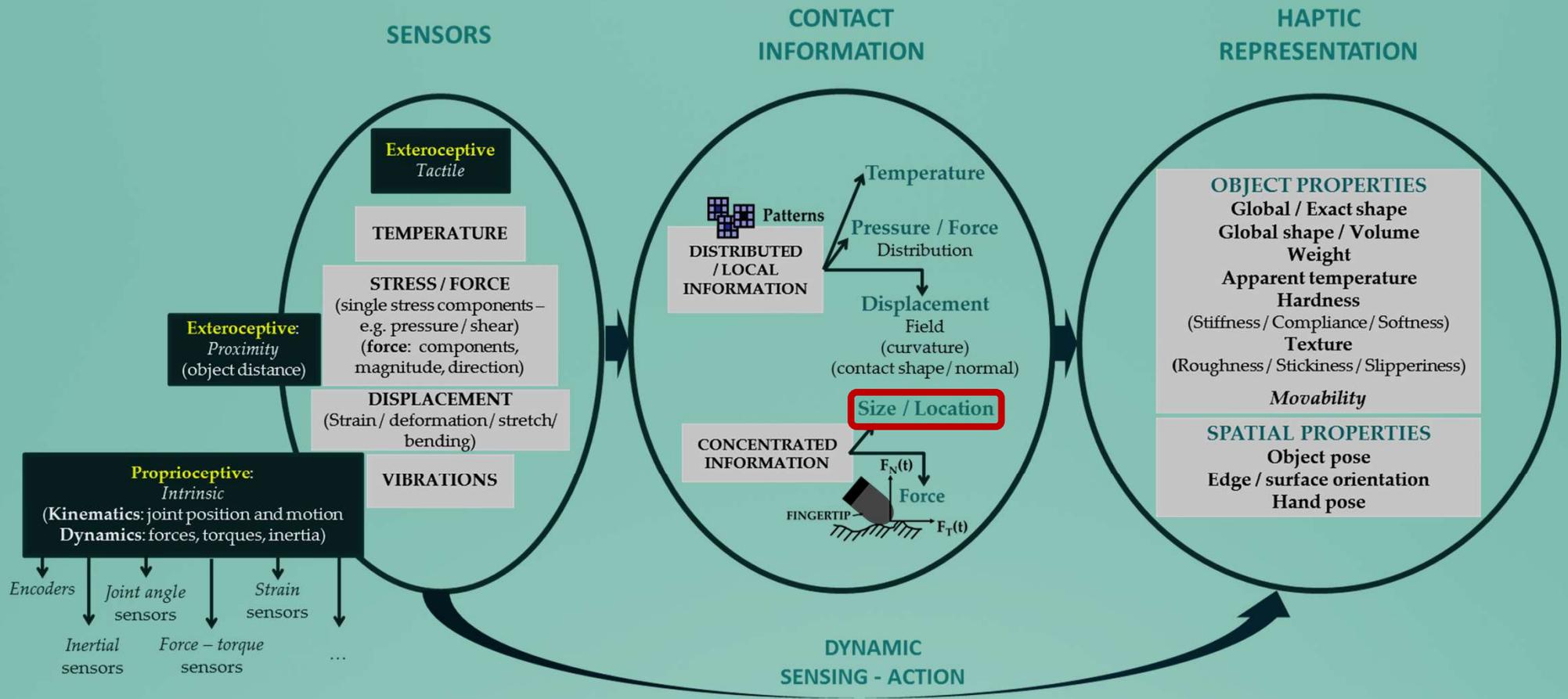
Signal processing at the taxel level?

OR

Rough signals?

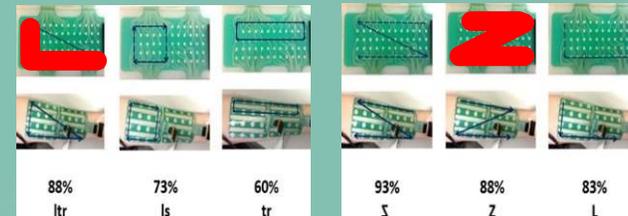
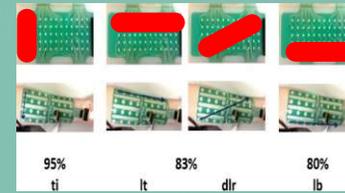
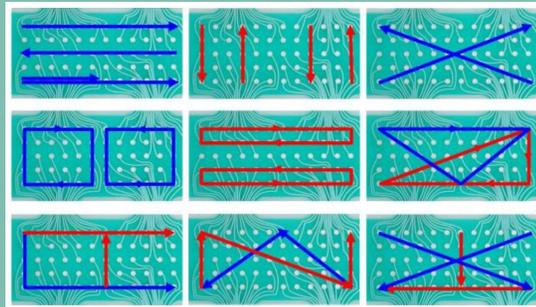


PROSTHETICS

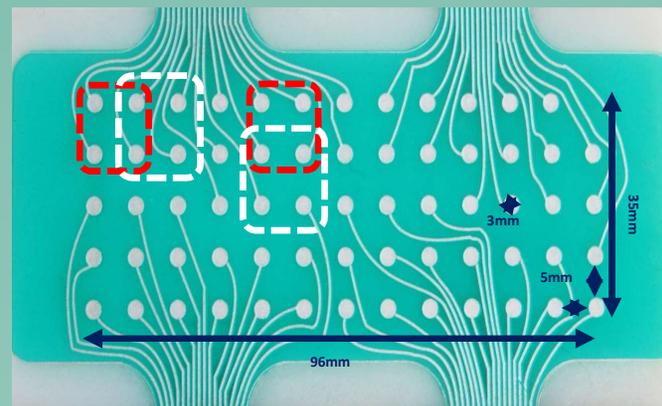


Seminara, L., Gastaldo, P., Watt, S. J., Valyear, K. F., Zuher, F., & Mastrogiovanni, F. (2019). Active haptic perception in robots: a review. *Frontiers in neurorobotics*, 13, 53.

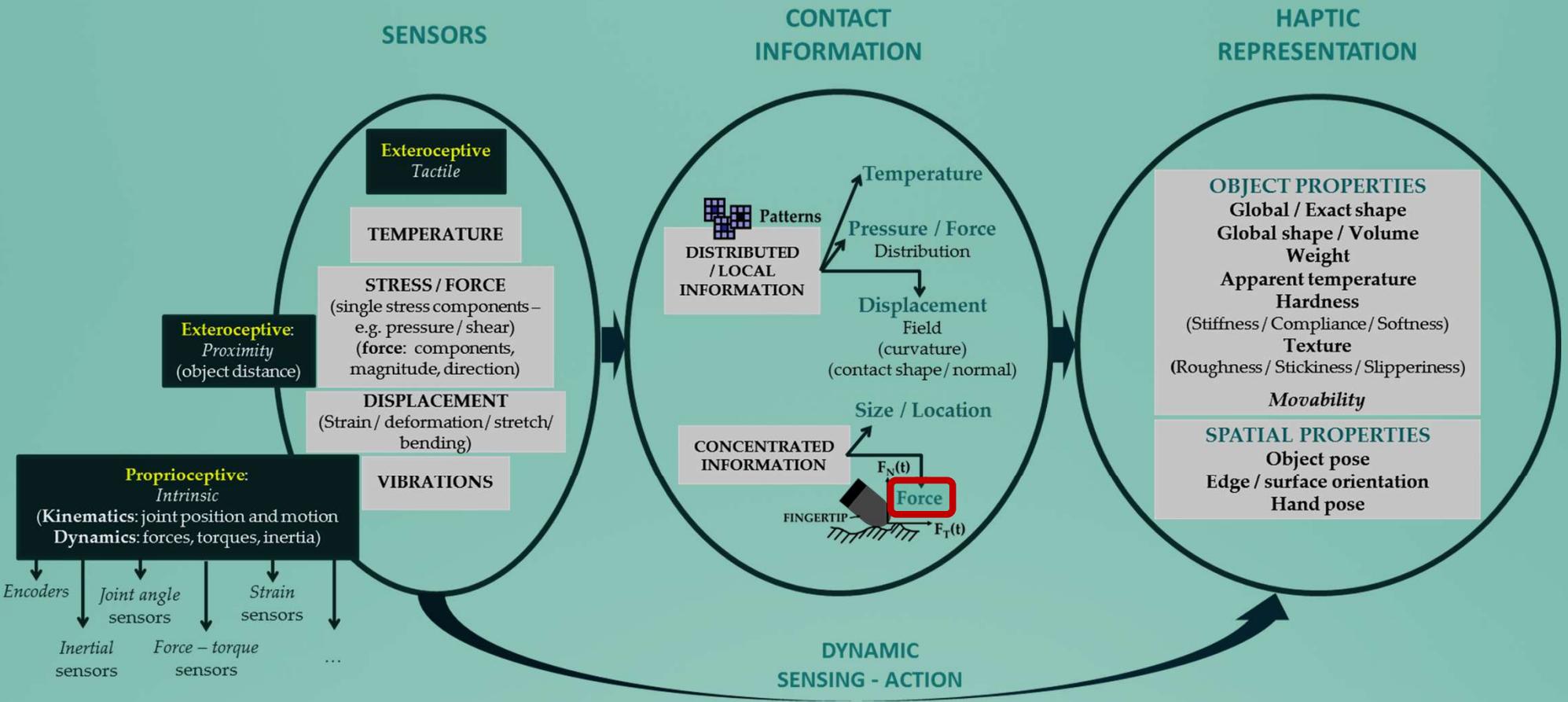
## Data processing (1): contact size, position and movement



### Space: Sensor fusion

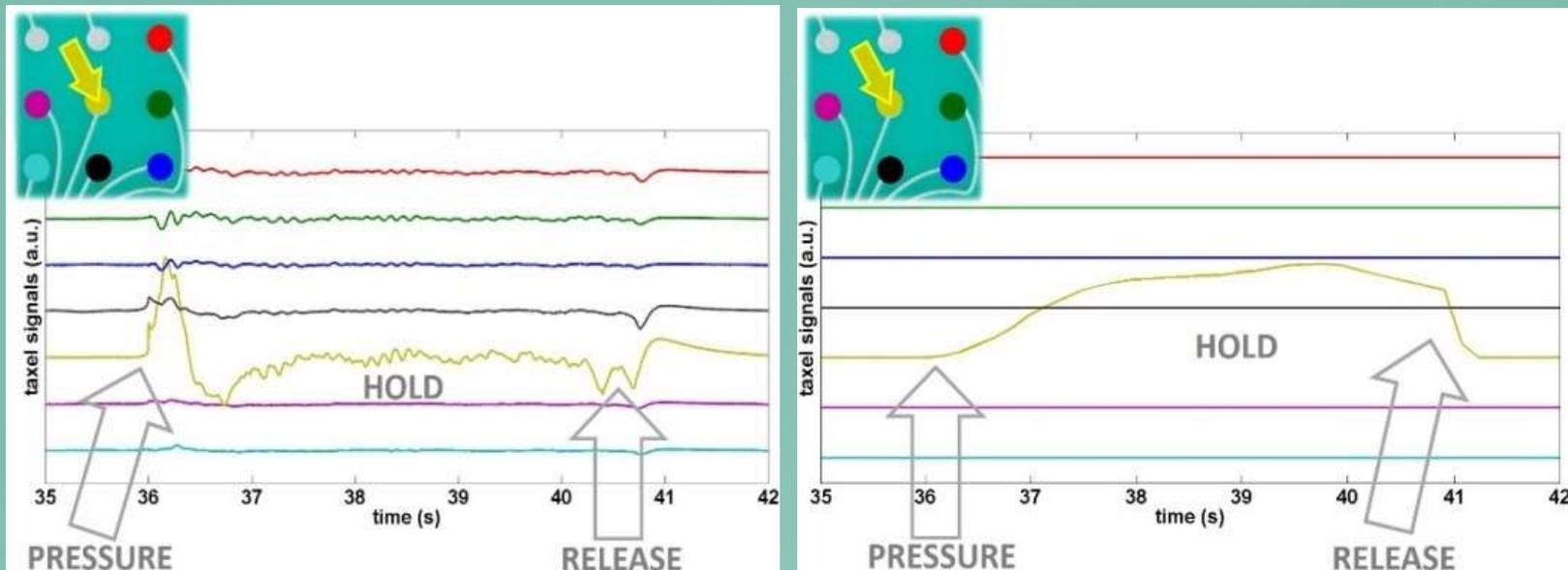


M. Franceschi, L. Seminara, S. Dosen, M. Strbac, M. Valle and D. Farina, "A System for Electrotactile Feedback Using Electronic Skin and Flexible Matrix Electrodes: Experimental Evaluation," in IEEE Transactions on Haptics, vol. 10, no. 2, pp. 162-172, 1 April-June 2017, doi: 10.1109/TOH.2016.2618377.

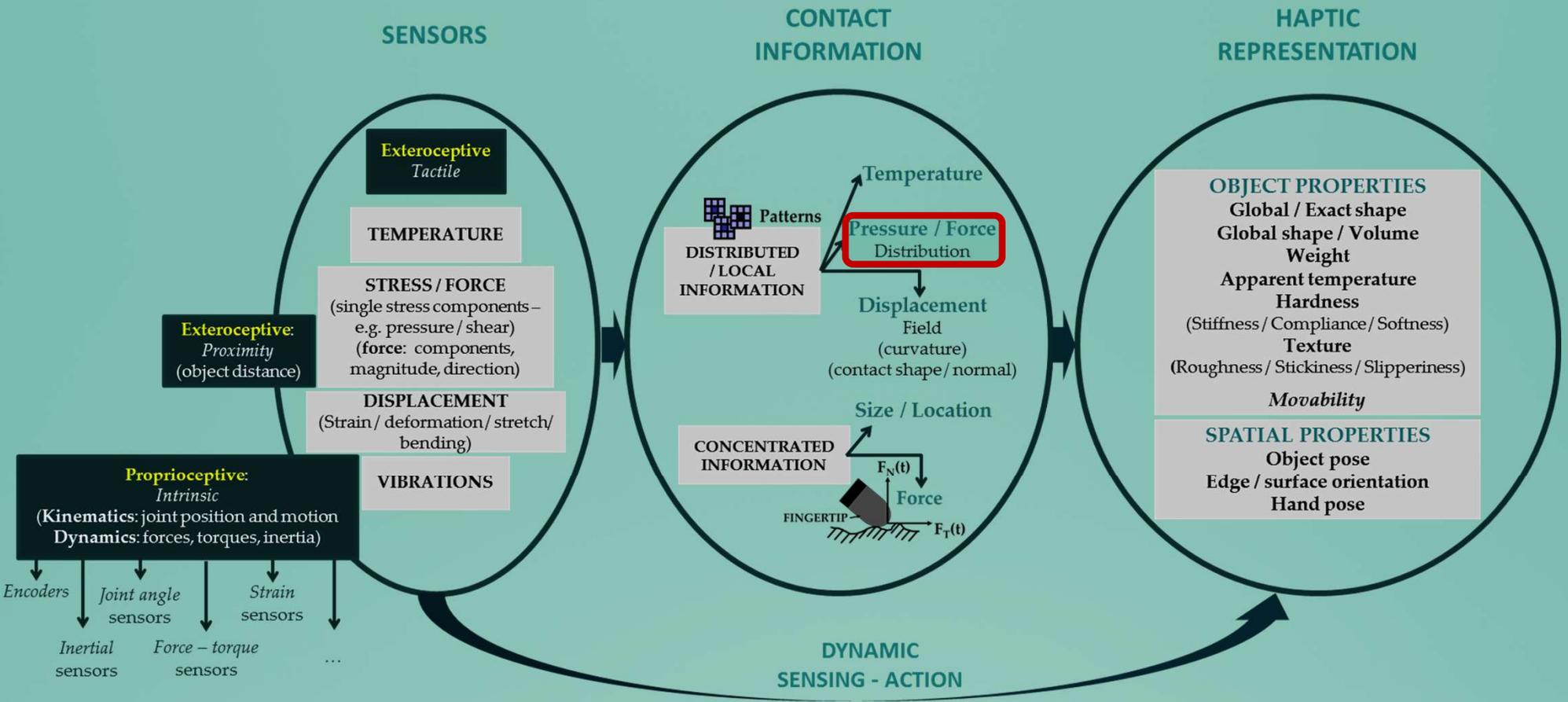


## Data processing (2): contact energy

*Time:* Integrative method



M. Franceschi, L. Seminara, S. Dosen, M. Strbac, M. Valle and D. Farina, "A System for Electrotactile Feedback Using Electronic Skin and Flexible Matrix Electrodes: Experimental Evaluation," in IEEE Transactions on Haptics, vol. 10, no. 2, pp. 162-172, 1 April-June 2017, doi: 10.1109/TOH.2016.2618377.

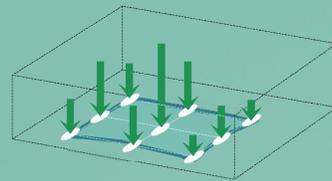


## Data processing (3): reconstruction of the contact force distribution

### Array structure:

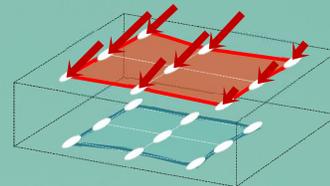
Normal stress component in the sensors: **MEASURED**

Surface force distribution + contact shape: **RECONSTRUCTED**



SENSOR  
GRID

RECONSTRUCTED  
CONTACT FORCE



SENSOR  
GRID

- ▶ Goal: from the **measured normal stress component** in the sensors, the goal is to reconstruct **complete contact force vectors** at **discrete points** on the upper surface layer.

## Proposed approach

- Discretize external forces
- Derive parameterized solutions *compatible with physical constraints*
- Parameters found to maximize an “efficiency” functional

### BOUSSINESQ'S EQUATION

$$\mathbf{n} \cdot \mathbf{T}(i) = \frac{3}{2\pi} \sum_j \frac{\mathbf{F}(j) \cdot \mathbf{r}(ji)h}{(\hat{r}^2(ji) + h^2)^{5/2}} \mathbf{r}(ji)$$

DIRECT PROBLEM:  $\mathbf{b} = \mathbf{C} \mathbf{x}$

Sensors only give information about the normal  $T_{33}$  component

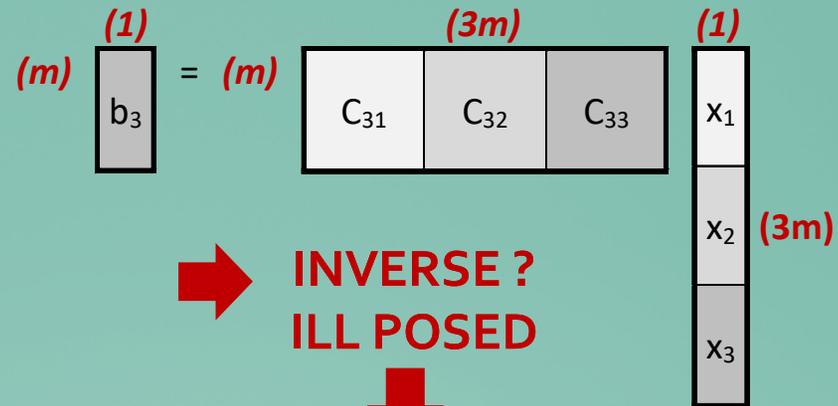
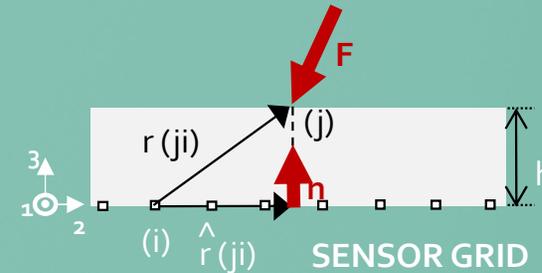
### BOUSSINESQ'S EQUATION

$$T_{33}(i) = \frac{3}{2\pi} \sum_j \frac{(\hat{\mathbf{F}}(j) \cdot \hat{\mathbf{r}}(ji) + F_n h)h^2}{(\hat{r}^2(ji) + h^2)^{5/2}}$$

Choice of the solution: The  $\mathbf{x}$  solution which is best complying with the physical conditions of the problem =  $\mathbf{x}$  vector contains the best (most “efficient”) 3-component force distribution.

## Assumptions

- Elastic half-space bounded by a plane
- Elastomer layer Poisson ratio  $\nu \sim 0.5$
- Small deflections

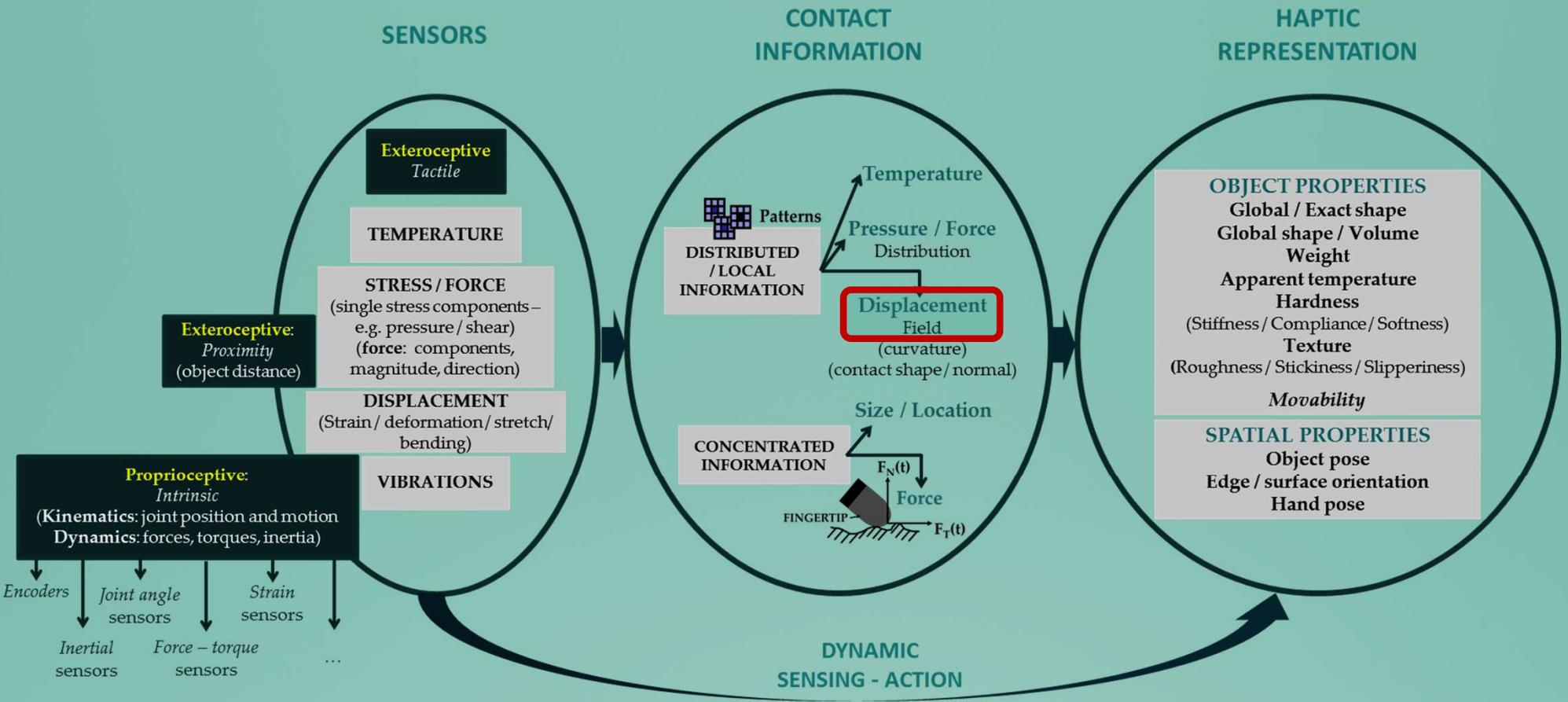


INVERSE ?  
ILL POSED

SET OF SOLUTIONS

$$\mathbf{x} = \mathbf{C}^\dagger \mathbf{b} + (\mathbf{I} - \mathbf{C}^\dagger \mathbf{C}) \mathbf{w}$$

[  $\mathbf{C}^\dagger = \mathbf{C}^T (\mathbf{C} \mathbf{C}^T)^{-1}$  MOORE-PENROSE PSEUDOINVERSE ]

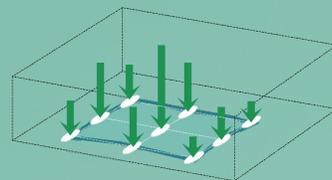


## Data processing (4): reconstruction of the displacement distribution (contact shape)

### Array structure:

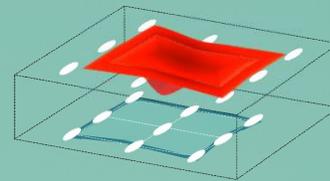
Normal stress component in the sensors: **MEASURED**

Surface force distribution + contact shape: **RECONSTRUCTED**



SENSOR  
GRID

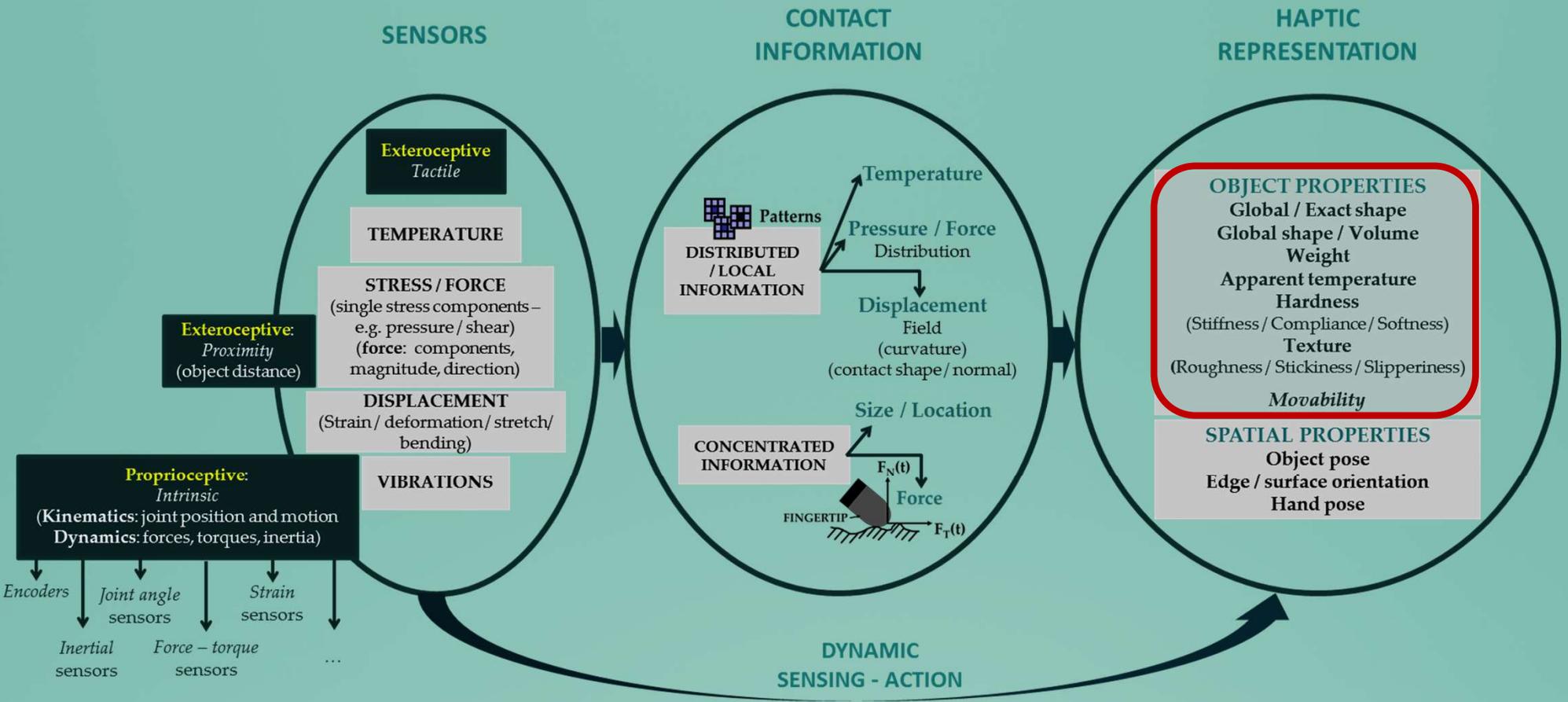
RECONSTRUCTED  
CONTACT SHAPE



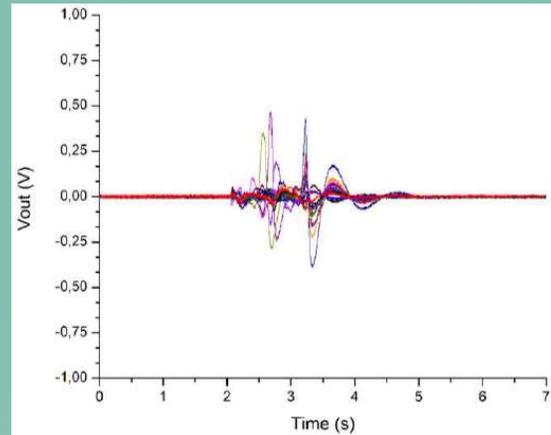
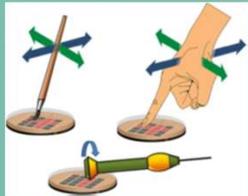
SENSOR GRID

- ▶ Goal: from the **reconstructed contact force vectors** calculate **displacements** at **discrete points** on the upper surface layer.

Muscari, L., Seminara, L., Mastrogiovanni, F., Valle, M., Capurro, M., & Cannata, G. (2013, May). Real-time reconstruction of contact shapes for large area robot skin. In 2013 IEEE International Conference on Robotics and Automation (pp. 2360-2366). IEEE.



## Data processing (5): classifying the touch modality



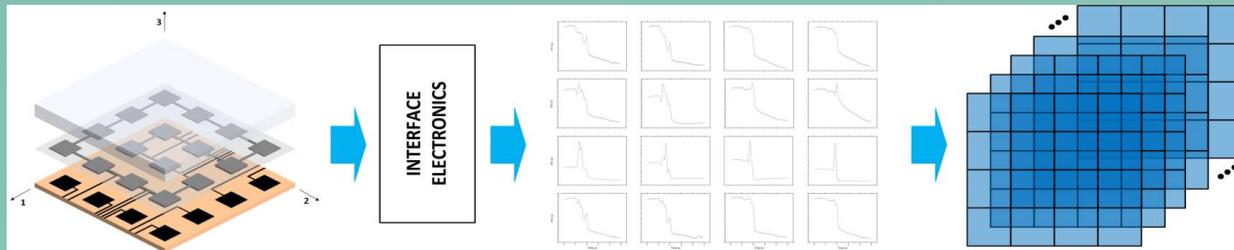
MACHINE LEARNING

Learning by examples

Offline Training  
Data

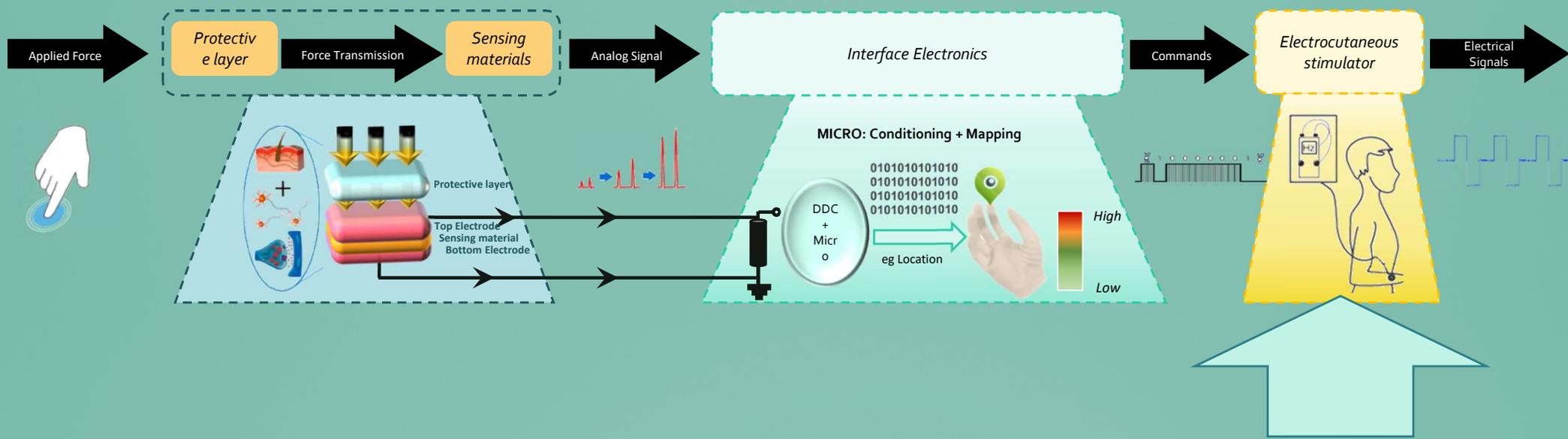
Online  
Data

Online  
Classification



Touch modality classification

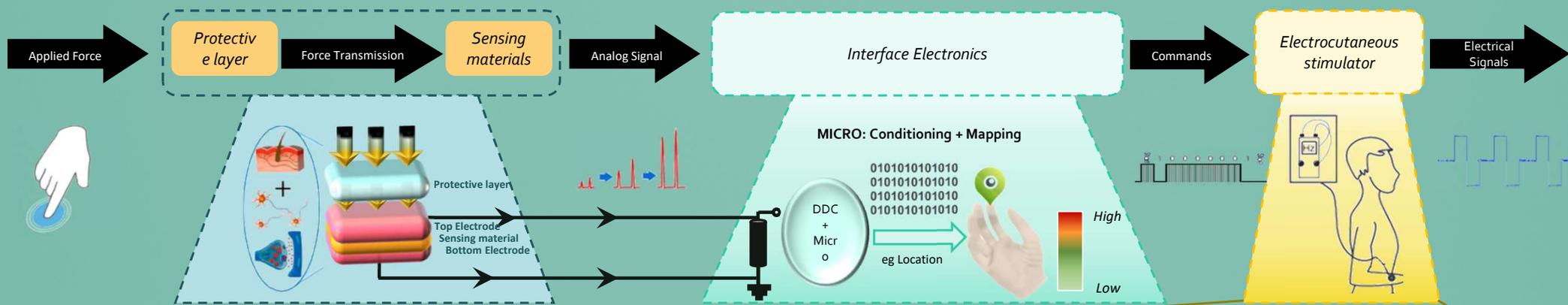
Gastaldo, P., Pinna, L., Seminara, L., Valle, M., & Zunino, R. (2015). A tensor-based approach to touch modality classification by using machine learning. *Robotics and Autonomous Systems*, 63, 268-278.



HIGH-DENSITY STIMULATION

FEEDBACK TO THE USER

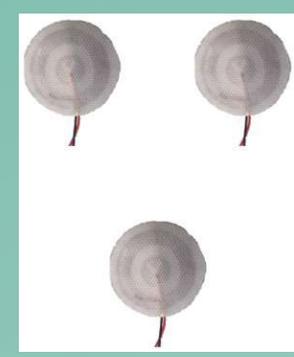
**The ability of perceiving  
movements on the skin  
and  
the spatial-temporal resolving  
capacity of the skin have an  
important role.**

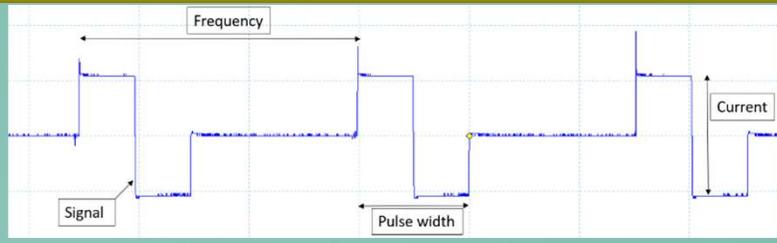


Electrocutaneous stimulator



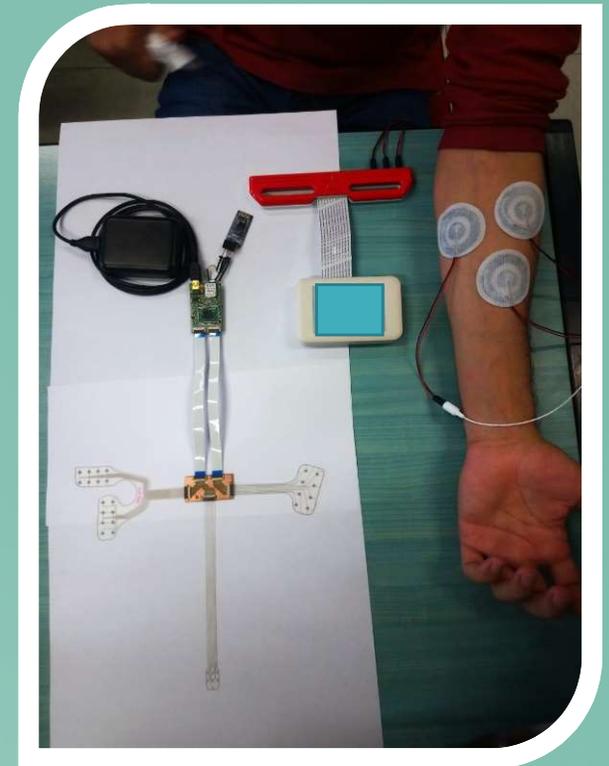
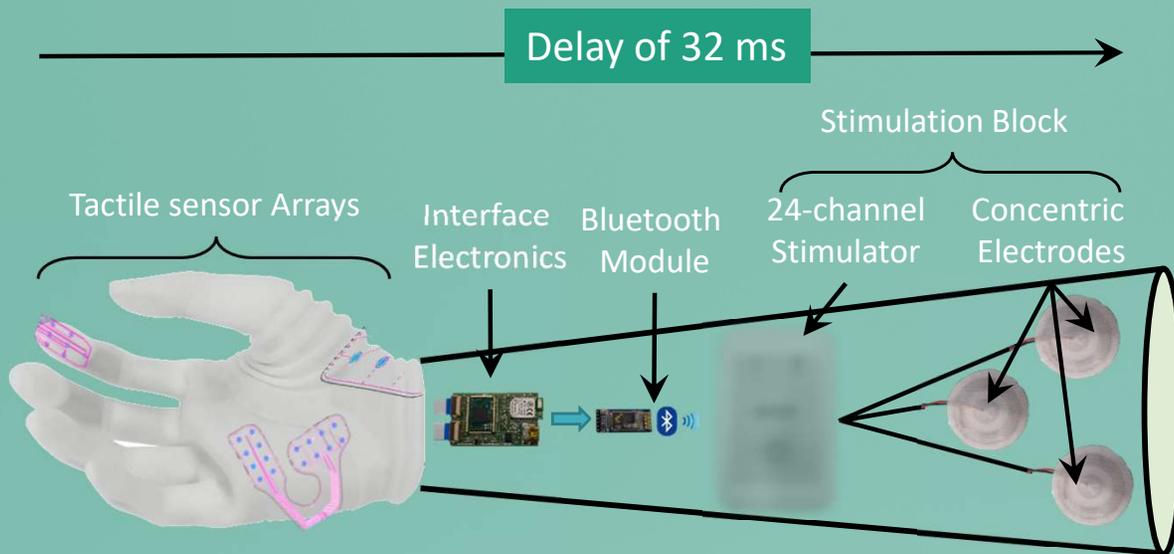
Concentric electrodes





- 24-channel programmable battery-powered stimulator
- charge-balanced biphasic continuous electrostimulation pulses  
 Current: 0-10mA with 0.1mA step.  
 Frequency: 1 to 400 Hz.  
 Pulse width: 50 to 500  $\mu$ s.
- self-adhesive concentric electrodes

# THE OVERALL SENSORY FEEDBACK SYSTEM



▶ MOTIVATION

▶ HUMAN SENSE OF TOUCH

▶ ARTIFICIAL SENSE OF TOUCH

- *Our system*: distributing sensing, electronics, cutaneous electrostimulation
- Clinical applications and *WORK IN PROGRESS*

# INTELLIGENCE ON THE PROSTHESIS

Autonomous management of  
vital – safety issues  
(*reflexive* behavior)

Feedback? What type?  
Autonomous when?  
EMBODIMENT

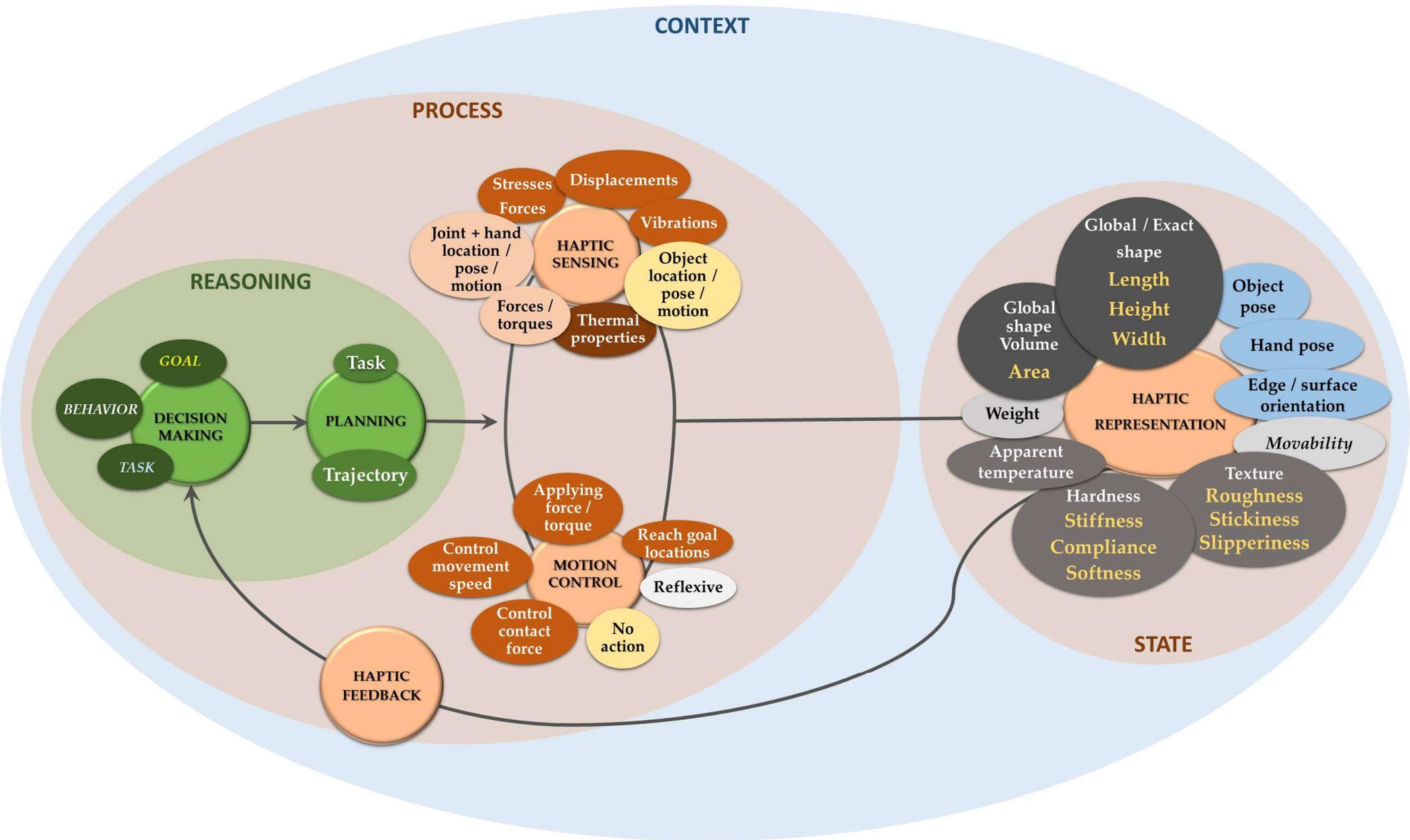
L. Seminara, S. Dosen, F. Mastrogiovanni, M. Bianchi, S. Watt, P. Beckerle, T. Nanayakkara, K. Drewing, A. Moscatelli, R. L. Klatzky and G. E. Loeb, (2023) A touch of humanity for human-in-the-loop artificial hands. Accepted for publication in SCIENCE ROBOTICS.

- ▶ Which kind of information about a touched object do we **send back to the user**? Only **low level or processed** or **“depending on user intention”**?
- ▶ How to convey this information back to the user? **What kind of feedback promotes embodiment?**
  - Where do we place electrodes?
  - Is that placing optimized on the specific task?
  - Which encoding? Frequency, power, amplitude...?



**TRAINING COUNTS!**

# THE BOTTLENECK IS STILL THE FEEDBACK INTERFACE



# COLLABORATIONS & ACKNOWLEDGEMENTS

Modeling mechanical behavior  
(Multiphysics / CAE simulations,  
analytical models)

*collab. Prof. Berselli, University of Genoa, Italy*

## Prosthetic application

*collab. Prof. Farina, Imperial College, UK*

*collab. Prof. Dosen, Aalborg University, Denmark*

From FPGA to ASIC  
Emerging techniques to reduce power consumption  
e.g. «Approximate Computing»  
Memory management («approximate memory»):  
*collab. Prof. Olivieri Univ. Roma 1*  
Implementation on Parallel Ultra Low Power (PULP) processors  
*collab Prof. Benini, ETH*  
Reducing Power Consumption of arithmetic blocks e.g.  
Tunable Floating Point multipliers: *collab. Prof. Nannarelli DTU*

## Embedded implementation

Art-science research center for studies  
related to touch

*www.tacta.it*

Spin-off activities related to Applications  
other than prosthetics: e.g. robotics,  
tele-operation, virtual reality

*collab. Prof. Dosen, Aalborg University, Denmark*

## Other applications

Other Applications in neurorehabilitation  
(rehabilitation of post-stroke patients)

*collab. Prof. Trompetto, Ospedale San Martino, Genova*

## Feedback side

Intuitive communication with the brain:  
**multisensory integration** as a framework  
*collab. Prof. Watt, Bangor University, Wales*

## Skin Integration



*collab. SMARTEX s.r.l., Prato, Italy*

## Hannes Hand

*Collab. De Michieli, Laffranchi, Boccardo, IIT, Genoa, Italy*



ANY  
QUESTIONS  
?